Detection of keratoconus in anterior segment photographed images using corneal curvature features

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ABSTRACT
Keratoconus is a corneal ectatic disorder with complex aetiology and may induce mild to severe visual impairment and consequently decrease the quality of life. This paper presents a new keratoconus detection method using corneal curvature features to differentiate normal and keratoconus cases. In this study, the eye images known as anterior segemented photographed images (ASPIs) are captured from side view using a smartphone’s camera. For the side-view images, the corneal curvature is segmented using spline function to measure the corneal curvature. A template disc method is implemented to quantitatively measure the steepening of the corneal curvature of the captured ASPIs. Parameters obtained from three different template disc methods, namely, nonlinear, $c_{nl}$, crossover point, $c_{cp}$, and trigonometric, $c_{tr}$, are investigated to represent the most suitable curvature feature. SVM is then employed to classify normal and keratoconus eyes. Results reveal that a standalone nonlinear method gives a reliable parameter with 90% accuracy in classifying the data. However, the classification performance has increased to 99.5% accuracy with the use of all combined features known as a feature vector, $f_c = \langle c_{nl}, c_{cp}, c_{tr} \rangle$. Additionally, classification with the proposed $f_c$ has successfully distinguished normal and keratoconus cases with sensitivity and specificity rates of 99% and 100%, respectively. The results portray the bright potential of this method in assisting experts during ocular screening specifically to detect keratoconus disease.

Keywords: Anterior segment, Corneal curvature, Keratoconus, Photographed images, Template disc

1. INTRODUCTION
Keratoconus (KC) is an ocular disease involving the progressive and non-inflammatory corneal thinning and steepening of the corneal curvature. However, the non-inflammatory condition has been questioned due to the existence of inflammatory components [1], [2]. The aetiology of KC is heterogeneous and varies widely depending on geographical factor, family history and races. The prevalence of this disease in the geographical locations of a country with hot climate is higher than that of a country with cooler climate. KC is also a hereditary disease. However, eye rubbing and allergy are the most consistent findings in contributions to the acceleration of corneal curvature advancement [3]-[6].
KC is an uncommon disease with 1 case out of 2000 individuals [7]; nonetheless, recent prevalence studies have shown major geographical variations, with the highest cases of 3.59% reported in Tehran [8] and...
the lowest prevalence of 0.00017% in Japan [9]. Despite this finding, only a few epidemiological studies have been performed in Asia, especially in Malaysia, because the focus was formerly on other diseases. Only one KC prevalence research has been conducted with a reported prevalence of 1.2% [10].

Several methods and equipment, such as placido disc, corneal topography and pentacam, can be used to diagnose KC. However, detecting the early phase of KC where the cornea looks relatively healthy is difficult. The latest extensive equipment includes corneal tomography, corneal biomechanics and in vivo confocal microscopy. These types of equipment, which can detect early signs of KC, provide detailed analysis of the corneal thickness and information on the corneal shape of anterior and posterior segment [11]. However, most of these types of clinical equipment are expensive, heavy and immobile and require experts or well-trained clinicians. In addition to using these types of equipment, ophthalmologists also manually refer to other clinical signs, such as in Rizzuti sign, Vogt striae and Munson [12] sign, as guidelines in diagnosing KC cases.

With the high pace of technology Internet of Things, researchers can integrate image processing techniques with smartphones via cloud computing. Tareq patented his work on the system and method for ophthalmological imaging using mobile processing device [13]. He developed a device which mimicked a topographical concept using a frustum cone segment, optimisation lens and vertex-angulation positioning light. To the best of our knowledge, only few works reported on KC detection approach using machine learning and image processing methods [13]-[16]. However, these works did not investigate the relationship of corneal curvature of ASPI and the presence of KC.

Numerous studies were conducted on other ocular disease detection methods [17]-[20] using image processing. Anterior segment photographed image (ASPI) is an image taken using a smartphone’s camera, a digital camera or any type of cameras. Nayak [21] proposed an automatic classification of normal, cataract and post-cataract of ASPIs using SVM classifier. The algorithm could classify correctly with nearly 90% accuracy. Raihanah et al. [22] proposed a screening system which can detect and classify pterygium and non-pterigium of ASPIs using image processing technique that was combined with machine learning algorithm. The system performed with accuracy of 95.6%. Masoud et al. [23] used the template disc method to calculate the tortuosity of retinal blood vessel of fundus images for an automated grading of diabetic retinopathy. They improvised the methods and produced the other two methods, namely, crossover point and trigonometric methods, which are adapted in this work.

A new method of KC detection was developed using the corneal curvature of ASPI. The corneal curvature calculated using template disc is presented in this paper. Qualitatively, corneal curvature measured from a side view of ASPI can be used as an indication of KC severity. The curvature of a side view of a patient’s eye image will be measured before validating the eye’s condition using a topography machine with an expert’s advice. The proposed method is explained in the next section, whereas the results and discussion are discussed in Section 3. Lastly, the conclusion summarises the entire work in Section 4.

2. PROPOSED METHOD
The proposed method consists of four parts; preprocessing, segmentation, feature extraction and classification as in Figure 1.

![Flow chart of keratoconus detection system](image)

2.1. Preprocessing
The ASPIs are captured from the side view of patients’ eyes using smartphone cameras. In this study, Huawei P9 and iPhone SE are used to capture the eye images collected from the Ophthalmology Department, Kuala Lumpur Hospital. A total of 106 normal images and 112 KC images are collected, and all
images are validated by a collaborative optometrist using Corneal Topography (CT). CT generates a different topography map in different eye conditions, such as on Figure 2 (a) and (c) for KC and normal eye, respectively. Topography map is a colour-based map, where cool colours (cyan to blue) denote flat curves, mild colours (green to orange) specify medium curvature and warm colours (red to black) present high curvature. The range of colour is dependent on the type of equipment. However, we only focus on processing the collected ASPIs using image processing approach.

Corneal is the transparent front structure of the eye. In normal corneas, the light scattering is minimal because of the transparency character; however, for abnormal corneas, the light scattering increases, and consequent loss of corneal transparency occurs [24]. Given this condition, ASPIs have noises such as reflection, uneven illumination and luminosity. Thus, gamma corrector technique is applied to the image during preprocessing to control the luminosity of ASPIs, thereby indirectly enhancing the edges of the cornea and reducing the reflection.

![Figure 2](image)

Figure 2. The side-view image of (a) KC eye with (b) topographical map, and (c) normal eye with (d) topographical map

2.2. Segmentation

Image segmentation is a partition of pixels into subregion to simplify the image into something that is remarkable. In this work, a semi-automated segmentation approach is performed by selecting the points \((x, y)\) around the corneal curve, as shown in Figure 3.

![Figure 3](image)

Figure 3. Corneal curvature segmented using Spline function

Spline linear interpolation is then used to connect the points with lines, which are the red line as shown in Figure 4. The selection must be on the edge of the curve with more than five coordinates.

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Our experiment shows that the best number of point selection is 10 points; nevertheless, more points chosen will yield more accurate curvature. Spline is a continuous function which interpolates the data between two points where it is constructed from linear functions interpolating polynomials. The red curve is then extracted to obtain the binary presentation as shown in Figure 4 b. Curvature measurement is calculated in the next section.

2.3. Feature Extraction – Estimation Curvature Calculation

Curvature is an indication of local twistedness of a curve [23]-[25]. Several methods exist for measuring curvature of a curve. The curvature is implied as an absolute value of curvature by not considering the rotation of the tangent. The parametric representation when coordinates \( x = x(t) \) and \( y = y(t) \) are given, [23]

\[
k = \frac{x'y' + x'y''}{[(x')^2 + (y')^2]^{3/2}}
\]  

(1)

This approach known as a template disc, where \( f(x) \) is a curve, in this case, refers to a corneas curve. A template disc of radius, \( d \) is created at the centre of the curve as in Figure 5 to calculate the curvature at a point \( (x, y) \).

The fundamental idea of this method is the relationship between the areas of the curve. The template disc of a suitable radius is placed with its centre at the particular point of the curve. Radius \( d \) should be smaller than radius \( r \). Mathematically, the position of the template disc and curvature imply the following:

\[
y = \frac{1}{2}cx^2 + O(x^3)
\]  

(2)

where \( c \) is curvature at origin and \( O(x^3) \) denotes higher order term. The normalisation in polar coordinates \((r, \theta)\) can be written as:

\[
R \sin \theta = \frac{1}{2}CR^2 \cos \theta + O(R^3 \cos^3 \theta)
\]  

(3)

where \( R = r/b \) and \( C = c/b \). Then, assume that \( \theta \approx 0 \)

\[
\theta(R) = \sin^{-1} \left[ \frac{1}{2}CR + O(R^2) \right]
\]  

(4)
The angle $\theta$ can now be denoted as the angle between the tangent line passing through the origin while area $A$ can be assumed as the area between the corneal curve and the disc as

$$a = \int_0^1 RdR \left( \frac{\pi - \theta(R)}{B(R)} \right) d\theta$$

(5)

where $a = Ab^{-2}$. Replaced 17164 (4) into (5) while ignoring the high order term and in terms of $c$ yield

$$c \approx \frac{3A_k}{d^2} - \frac{3\pi}{2d}$$

(6)

where $A_k$ is the complement of $A$. Hence 17164 $c \propto A_k$ and nonlinear estimation of a curve is defined as

$$c_{nl} \triangleq A_c$$

(7)

The hypothesis of this work is that the more convex of the cornea, the more severe the KC cornea is. Quantitatively, high $A_c$, indicates the high severity of KC. On the basis of [23], Masoud et al. claimed that this method becomes inaccurate when the concern was high estimation curvature. Therefore, through its simplicity, Masoud modified the method using the crossover point, $c_{cp}$ at $\theta_c$ and trigonotrimetrical method, $c_{tr}$. The approximations of curvature are as follows

$$c_{cp} \triangleq \frac{1}{A^2}$$

(8)

$$c_{tr} \triangleq \frac{2\sin \theta_c}{\cos^2 \theta_c}$$

(9)

We adapt the three features $c_{nl}$, $c_{cp}$ and $c_{tr}$ into one feature vector, $f_c = [c_{nl}, c_{cp}, c_{tr}]$. The feature of $c_{nl}$ and $c_{cp}$ is a form of integration which only rely on area calculation; thus, these features are robust and yield smooth results. The comparison is discussed in the next section.

2.4. Classification

Before the evaluation of the proposed methods, one-way analysis of variance (ANOVA) is employed to determine the statistically significant values between normal and KC corneal curvatures. ANOVA is a statistical method used to find the optimum feature and the existence of significant difference between sets. The results show that only $f_{e1} = [c_{nl}]$ for the left eye is not significant ($p=0.884$), as bolded in Table 1, whereas that for right eye is significant ($p<0.05$) for all features. Thus, all features are fed into Support Vector Machine (SVM) classifier.

The classification of corneal curvature is tested using SVM and decision trees. SVM is a type of pattern classifier based on a novel statistical learning technique [21]. This step is crucial to analyse the curvature either normal or KC. Moreover, this step will evaluate the distinctiveness of the approached algorithm.

<table>
<thead>
<tr>
<th>Features</th>
<th>Right</th>
<th>Left</th>
</tr>
</thead>
<tbody>
<tr>
<td>$f_{e1} &lt; c_{nl}$</td>
<td>1.64E-02</td>
<td>8.84E-01</td>
</tr>
<tr>
<td>$f_{e1} &lt; c_{cp}$</td>
<td>3.60E-07</td>
<td>3.40E-07</td>
</tr>
<tr>
<td>$f_{e1} &lt; c_{tr}$</td>
<td>4.80E-08</td>
<td>1.30E-06</td>
</tr>
</tbody>
</table>

Three standalone features $f_{e1} = [c_{nl}]$, $f_{e2} = [c_{cp}]$, $f_{e3} = [c_{tr}]$ and four combined features vector $f_{e12} = [c_{nl}, c_{cp}]$, $f_{e13} = [c_{nl}, c_{tr}]$, $f_{e123} = [c_{cp}, c_{tr}]$, $f_{e} = [c_{nl}, c_{cp}, c_{tr}]$ are used to classify the corneal curvature. Training images are fed into the SVM classifier for training. The trained classifier predicts the testing database without knowing the class of the image. Kernel-based functions include linear kernel function, polynomial kernel function, Gaussian Kernel and Radial Basis Function (RBF). After several testing and experimental on the training data using polynomial kernel function, cubic kernel function is selected in SVM for classification where the input data are transformed into high dimensional space to become discrete compared with the original space.

$$K(x, y) = (x, y + 1)^p$$

(10)
where \( p \) is a tunable parameter; for cubic kernel, \( p=3 \).

A decision tree is an array of “if-then-else” rules for allocation class label to exemplify the data set in the form of tree structure [26]-[27]. A decision node consists of two or more branches, whereas a leaf node represents a decision. The process of developing a tree involves three steps: (a) splitting the data set into subsets, where 4 number of splits are made; (b) pruning is truncating the branches and (c) tree selecting is finding the smallest tree that yields the lowest cross-validated error. The deeper the tree, the fitter the model with more complex of decision rules is. However, the tree must prune the data well; otherwise, it might be over-fitting, which leads into false classification. We use simple decision tree, and the performance results are discussed in the next section.

3. RESULTS AND DISCUSSION

The local dataset consisting of 218 images is used to test the reliability of the proposed algorithm using four main steps as explained in Methodology section. The normal and KC ASPIs include the left and right eyes captured from the side view. For these side-view images, the corneal curvature is segmented using spline function to measure the corneal curvature before significant features are extracted. Figures 6 and 7 present the results of 218 images, both eyes, classified using SVM and decision tree. Both classifiers are applied in this work using the standalone and combinations features, \( <c_{\text{nl}}, c_{\text{cp}}, c_{\text{tr}} > \): nonlinear estimation, crossover point and trigonometrical methods. The SVM classifier performs well with the two-combined features \( f_{c12} = < c_{\text{nl}}, c_{\text{cp}} > \) for both eyes with average accuracy of 98.4% (Figure 6) compared with standalone feature \( f_{c1} = < c_{\text{nl}} > \) and \( f_{c2} = < c_{\text{cp}} > \) which is only below than 90%. The weakest combination is \( f_{c23} = < c_{\text{cp}}, c_{\text{tr}} > \) for right eye with 72.6% and for left eye is 65.4%. Overall, the SVM achieves 99.5% accuracy for both eyes; whereas the decision tree only attains 96.3% and 83.8% for right and left eyes, respectively, with the combination of all features \( f_{c} = < c_{\text{nl}}, c_{\text{cp}}, c_{\text{tr}} > \). Hence, the corneal curvature method is reliable and competent to classify the KC and non-KC eye using SVM classifier.

![Figure 6. Percentage of accuracy for each and combination features classified using SVM](image1.png)

![Figure 7. Percentage of accuracy for each and combination features classified using decision tree](image2.png)
The sensitivity of the approach method is 99%, and the specificity is 100%. In this context, sensitivity indicates that the algorithm can classify the KC disease in KC group; whereas the specificity specifies that the system is competent to classify the non-KC disease in normal group. However, only one case of KC classified in normal group is identified as false negative. The overall performance of this system is reliable in detecting KC eye.

4. CONCLUSION
A new detection method for KC was proposed using local database and four new modules, namely, preprocessing, feature extraction, segmentation and classification. ASPI was captured from side view of an eye image, and the corneal curvature was calculated using the three parameters of template disc method, namely, nonlinear, crossover point and trigonometrical method. The feature vector, \( f_c = < c_{AL}, c_{EP}, c_{TV} > \) was then fed into SVM to classify the eye images with accuracy of 99.5%, sensitivity of 99% and specificity of 100%. This system may provide a screening platform for KC detection cases namely people living in rural area, where ophthalmologists are hard to be reached. In line with that purpose, an automated segmentation approach should be developed to produce a user-friendly system in assisting experts during the corneal examination.

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Marizuana Mat Daud is a PhD candidate at Universiti Kebangsaan Malaysia. Her research interests include image processing with machine learning focusing on biomedical field. More specifically, her work examines how image processing with machine learning techniques could contribute towards better and more efficient ways of analyzing and understanding medical images. Apart from that, her research interest also includes assistive technologies for people with disabilities.

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Aini Hussain obtained her B.Sc. in Electrical Engineering from Louisiana State University (LSU), Baton Rouge, USA; M.Sc. in Systems and Control from the University of Manchester Institute of Science and Technology (UMIST), Manchester, U.K., and Ph.D. in Electrical and Electronic Engineering from the National University of Malaysia in 1985, 1991 and 1997, respectively. She is a Professor and currently, the Chair of the INTEGRA research center also known as “Centre for Integrated Systems Engineering and Advanced Technologies”. Her research, for which she has received funding, focuses on Intelligent Systems and Image Processing. Her current research interests are in machine learning, pattern recognition and video & image processing.

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